

Diffusion Smoothing on the Cortical Surface

Moo K. Chung*, Keith J. Worsley**†, Jonathan Taylor*, Jim Ramsay†, Steve Robbins†, Alan C. Evans†

*Department of Mathematics and Statistics

†Montreal Neurological Institute

‡Department of Psychology, McGill University

Abstract

Gaussian kernel smoothing has been widely used in either 2D flat or 3D volume images, but it does not work on the curved cortical surface. However, by reformulating Gaussian kernel smoothing as a solution to a diffusion equation on a 2D manifold, we can generalize it to the cortical surface. This generalization is called *diffusion smoothing* and has been used in analysis of fMRI data on the cortical surface [1] and detecting cortical surface-area growth [3]. We give an exact mathematical formulation for the diffusion smoothing on *triangulated* cortical surfaces so that this technique can be used for any surface-based functional and structural analysis. As an illustration, we smooth the mean curvatures on the outer cortical surfaces to show how the the smoothing actually incorporates the geodesic curvature information of the surface.

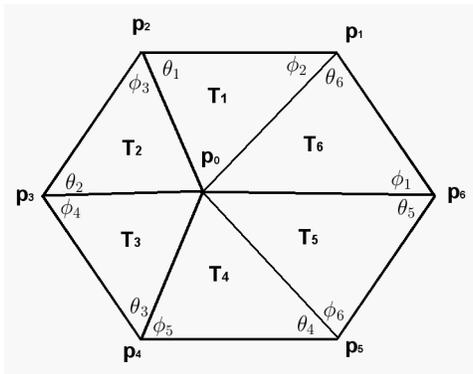


Figure 1: A typical triangulation

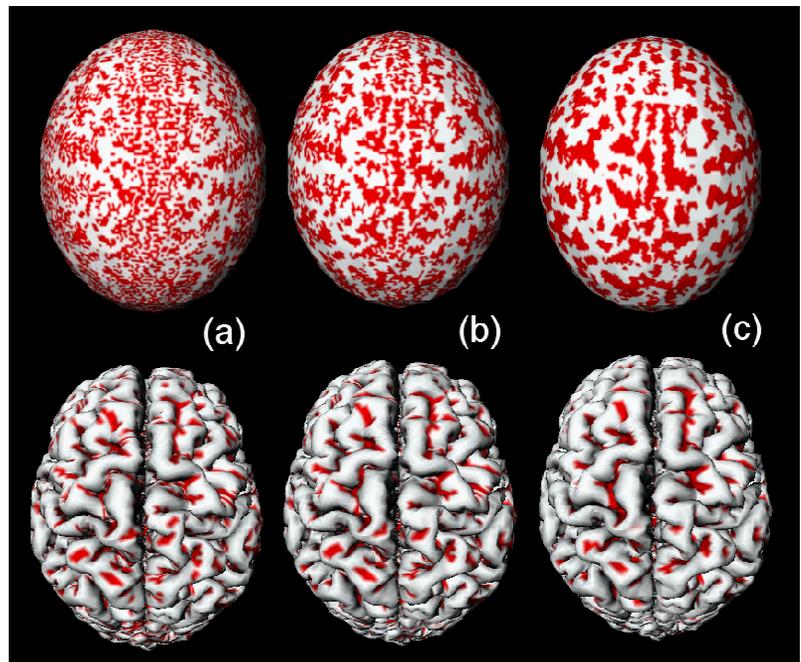


Figure 2: The mean curvature from the outer cortex is mapped onto an ellipsoid during the diffusion smoothing. (a) Before the iteration (b) After 40 iterations (c) After 100 iterations

Methods

Gaussian kernel smoothing of the signal $f(x)$ in n -dimension with $\text{FWHM} = 4(\ln 2)^{1/2} t^{1/2}$ is defined as the convolution of the n -dimensional Gaussian kernel $G(x;t)$ with the signal $f(x)$, i.e. $F(x,t) = f * G(x;t)$. It can be shown that the convoluted signal F is the solution of a diffusion equation $dF/dt = L[F]$ with the n -dimensional Euclidean Laplacian L . Since the cortical surface is non-Euclidean, the Euclidean Laplacian is not well defined on the cortical surface. The generalization of the Laplace operator L to an arbitrary curved surface is called the *Laplace-Beltrami operator* and it is defined in terms of the Riemmanian metric tensors.

In order to estimate the Laplace-Beltrami operator on a triangulated cortical surface, we have used the *finite element method* [2]. Let $F(p_i)$ be the signal on the i -th node p_i in the triangulation. If p_1, \dots, p_m are m -neighboring nodes around $p = p_0$, the Laplace-Beltrami operator at p is estimated by

$$L[F(p)] = w_1(F(p_1) - F(p)) + \dots + w_m(F(p_m) - F(p))$$

with the weights $w_i = (\cot \phi_i + \cot \theta_i) / (T_1 + \dots + T_m)$, where ϕ_i and θ_i are the two angles opposite to the edge $p_i - p$ in triangles and $T_1 + \dots + T_m$ is the sum of the areas of m -incident triangles at p (Figure 1). Then the diffusion equation is solved via the *finite difference scheme*:

$F(p_i, t_{n+1}) = F(p_i, t_n) + (t_{n+1} - t_n) L[F(p_i, t_n)]$ with the initial condition $F(p_i, t_0) = f(p_i)$. After N -iterations, the diffused signal is locally equivalent to the Gaussian kernel smoothing with $\text{FWHM} = 4(\ln 2)^{1/2} N^{1/2} (t_n - t_0)^{1/2}$ [2].

Results

The ASP method [3] is used to extract the outer cortical surfaces each consisting of 81920 triangles from MR scans. At this surface sampling rate, the average intervertex distance is about 4mm. The mean curvature $f(p_i)$ of the cortical surface is computed based on the least-squares estimation of a local quadratic surface [2]. Figure 2 shows the diffusion smoothing of the mean curvature with 5mm FWHM. If the smoothing were based on simple inter-nodal averaging, such sulcal pattern is not possible to obtain.

Conclusion

Gaussian kernel smoothing can be generalized to cortical surfaces enabling surface-based statistical analysis. The numerical implementation will be freely available as Matlab code on the web at <http://www.math.mcgill.ca/keith/BICstat>.

References

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